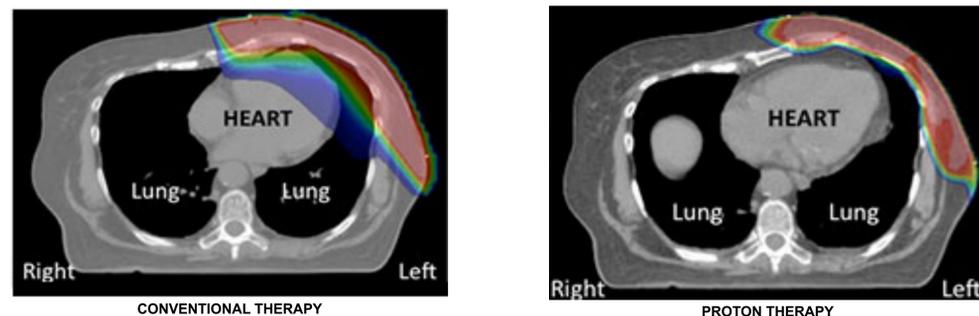


## I. INTRODUCTION

- Systemic therapy with large-field radiotherapy (RT) to the chest wall and lymph nodes in the mediastinum and axilla yields a substantial survival benefit,<sup>1</sup> but can result in inadvertent exposure of large volumes of normal tissues to low and moderate doses of radiation.
- There is a 7% increase in the relative risk of cardiac events with each 1-Gy increment in mean heart dose, for a 27% total increased relative risk for the typical patient.<sup>2</sup>
- Left-sided breast cancer patients who receive RT to the chest wall have a 4-fold higher lifetime risk of cardiac events than patients with right-sided breast cancer who receive RT to the chest wall.<sup>3</sup>
- Because cardiac injury is a known risk of treatment, early markers of heart injury could be beneficial for follow-up management in these patients and may help identify new techniques that would improve the therapeutic ratio of treatment.



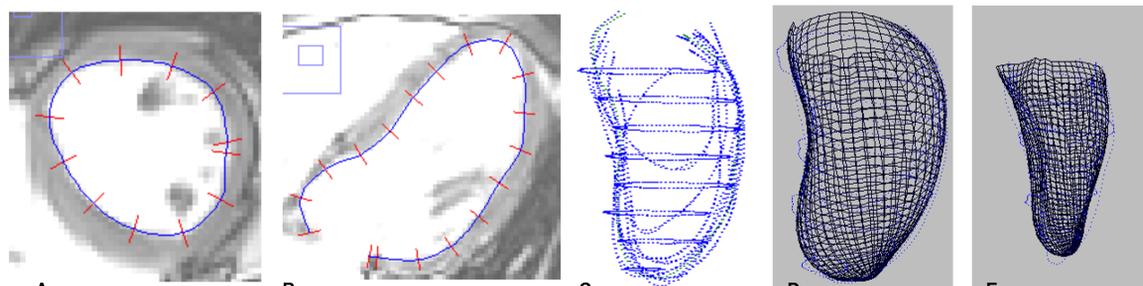
**Figure 1: Treatment Plans for Photon vs Proton Therapy:** Shown on the left is a conventional X-ray-based radiation treatment plan for a representative left-sided breast cancer patient. The color range from purple to yellow represents low to high radiation exposure. Shown on the right is a proton therapy plan for the same patient using similar constraints for target dose and dose to the heart and other organs at risk.

**OBJECTIVE :** To quantify subclinical changes in heart function and regional myocardial strains using cardiac magnetic resonance (CMR) images with cardiac tagging to compare risk of cardiac toxicity for standard X-ray based RT versus proton therapy treatment in breast cancer patients.

## II. METHODOLOGY

### IMAGE ACQUISITION

- CMR images were acquired at 8 to 10 time-frames over the systolic phase of the cardiac cycle in patients with left-sided breast cancer. Eight to 10 short- and long-axis views were acquired before and 6-12 months after completion of RT. Contrast-enhanced images were obtained to assess left ventricular volume and ejection fraction (LVEF). CMR images with parallel tags were acquired for wall strain analysis.



**Figure 2. Cardiac MR Images, contour segmentation, and surface fitting:** [A] and [B] show representative short- and long-axis CMR images with vascular contrast, overlaid with snake-based endocardial contours. [C] shows the contour points from all slices and views at time 0 (end-diastole). [D] and [E] show endocardial surface meshes generated from the surface models at end-diastole and end-systole, respectively, in the same patient and at same size scale.

### HEART LEFT VENTRICLE CONTOUR SEGMENTATION AND CAVITY VOLUME CALCULATION

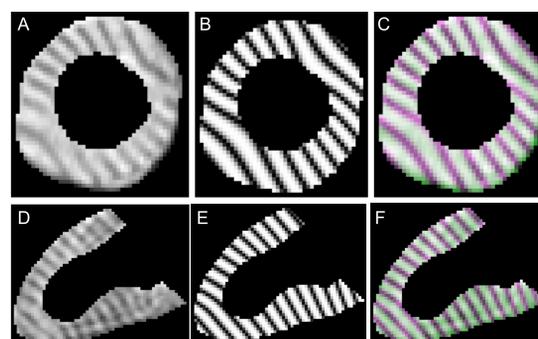
- An in-house semi-automatic snake based contouring toolkit was used to segment the left ventricular endocardial and epicardial borders on each image slice and time frame (Fig. 2A-C). Mathematical models for each surface were defined in a prolate spheroidal coordinate system with  $\lambda$ , the radial coordinate, expressed as a series expansion in  $\theta$  and  $\mu$ , the circumferential and longitudinal angles (Fig. 2D,E).
- Care was taken to demark the mitral valve ring as the first and last contour points in each long-axis view (Fig. 2B).

### DEFORMABLE IMAGE REGISTRATION AND STRAIN CALCULATIONS

- The motion of the heart was modeled by modes of deformation defined in the local heart-aligned, prolate spheroidal coordinate system, followed by the bulk motions: 3 rotations and 3 translations in x, y and z.
- Virtual tagged images were deformed according to the model parameters and compared with the patient MR images to determine the contribution of each mode and bulk motion.<sup>5,6</sup>
- A 3D mesh of material points was generated with 5 layers radially, 6 longitudinally, and 8 circumferentially. The 3D Lagrangian strain tensor,  $E$ , and fractional wall thickening,  $T$ , was calculated at each mesh point at multiple time points throughout the cardiac cycle.

### MAPPING RADIATION DOSE TO THE HEART WALL

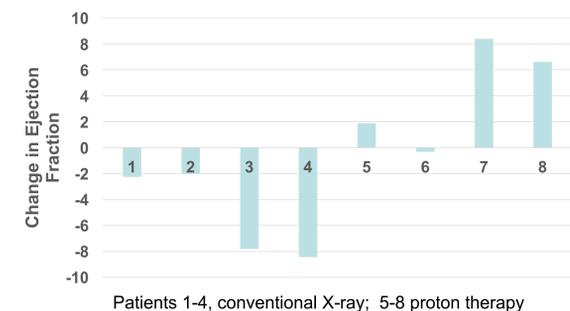
- Rigid body registration in 3D was performed to align the CT-based masks of the lung onto axial MR-based masks of the lung.
- The 3D dose field from the treatment planning system was subsampled to match the planning CT and axial MRI voxel locations.
- The dose at each material mesh point was interpolated from the nearest MRI voxels to correlate regional dose with wall mechanical strain.



**Figure 3. Modeling the deformation of parallel-tagged MR images:** [A] shows a tagged short-axis MR image at end-systole after applying a cropping to the segmented endo- and epi-cardial contours. [B] shows the deformed virtual tagged image at the same slice location and time. [C] shows a color overlay where green highlights the tags in the patient MR image, pink tags in the virtual image, and darker pink results when they are well-aligned.

## III. RESULTS

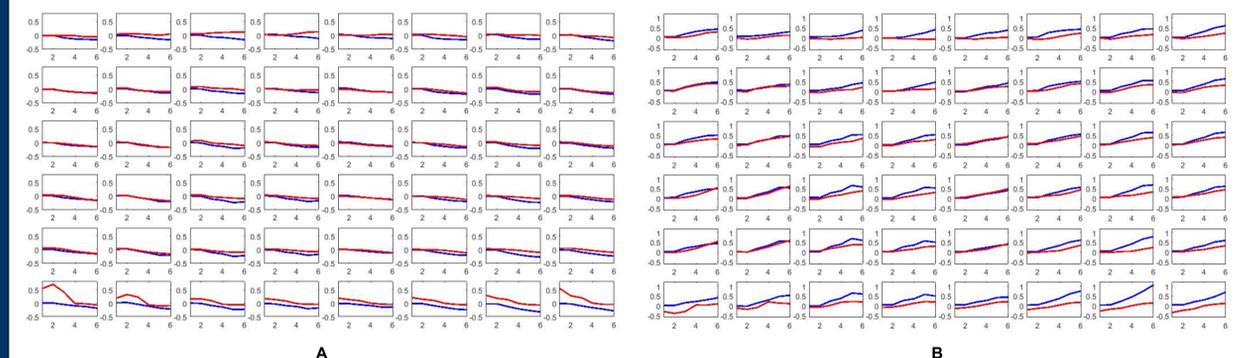
### LEFT VENTRICULAR VOLUME AND EJECTION FRACTION:



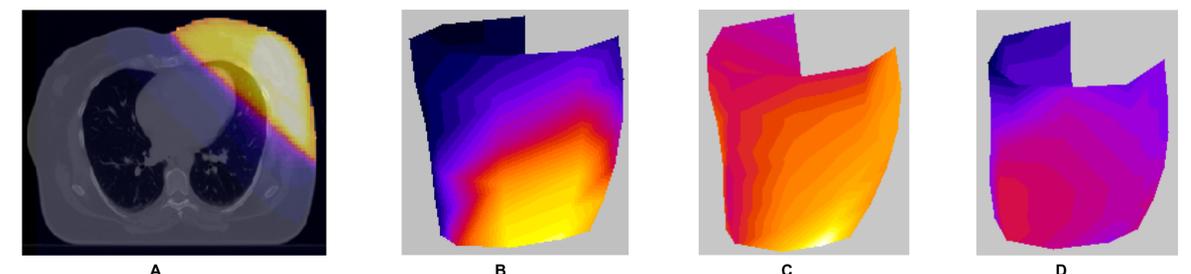
- Data sets from 4 conventional and 4 proton therapy patients were contoured at end-diastole and end-systole by an investigator blinded to the treatment modality.
- The mean left ventricular ejection fraction (LVEF) for the 4 conventional RT patients (#1-4) was 60% before treatment and 54.87% after treatment.
- For the 4 PT patients (#5-8), the mean LVEF was 57.54% before treatment and 61.68% after treatment.
- The difference in mean change in LVEF for conventional RT (-5.13%) and proton therapy (+4.15%) patients was significantly different ( $p < 0.05$ ).

### LEFT VENTRICULAR WALL MECHANICAL STRAIN:

- Regional wall strain was computed at pre-treatment and 12-months post-treatment in a conventional RT patient.
- A statistically significant decrease in magnitude of both mean circumferential and thickening strains at end-systole were found ( $p < 0.05$ ) post-RT compared with pre-RT.



**Figure 4. Circumferential strain and wall thickness multi-plots:** The multi-plots in [A] and [B] show strain computed at 8 circumferential (columns) and 6 longitudinal (rows) locations around the heart left ventricle. The circumferential position starts at the mid-septum (first column) and wrapping to the free wall (4<sup>th</sup>-5<sup>th</sup> columns) and back (8<sup>th</sup> column). The longitudinal level in the heart, from base to apex, varies from the top row to the bottom row. Each mini-plot shows strain on the vertical axis as a function of time on the horizontal axis, from end-diastole to end-systole. Only radial-mid-wall strains are shown. The multi-plot in [A] presents the evolution of circumferential strain, where more negative values indicate stronger contraction. [B] presents the evolution of wall thickening strain where more positive values indicate stronger contraction. The blue curves are for the pre-RT heart, and the red curves the post-RT heart.



**Figure 5. Heart dose calculation :** [A] shows the radiation dose on a planning CT image showing elevated exposure to the anterolateral left ventricular wall and apex. [B] shows the dose distribution overlaid onto the 3D mesh of mid-wall material points. The yellow region indicates high radiation exposure while black indicates low exposure (range 2 to 47 Gy). [C] and [D] show mid-wall thickening strain at pre-RT and post-RT, respectively, with color scaled from 0 (black) to 1.0 (white). This is the color 3D rendering of the data of Figure 4B. Thickening strain is diminished over the entire heart, with larger apparent decrease in the regions with higher dose.

## III. CONCLUSIONS & DISCUSSION

- A significant decrease in LVEF at 6 to 12 months post-RT was found in patients receiving conventional X-ray therapy compared with proton therapy.
- A significant decrease in heart wall circumferential and thickening strains was found post-RT in a patient receiving conventional X-ray therapy.
- These analysis techniques and initial findings are hoped to motivate and precipitate the pursuit of key clinical questions such as:
  - Does proton therapy improve the therapeutic ratio of breast cancer radiation treatment via reducing the severity of radiation toxicity to the heart?
  - Is there a role for cardiac imaging in routine clinical follow-up care of breast cancer patients for management of cardiac toxicity?
  - Can we identify breast cancer survivors that are at an elevated risk for cardiac disease who may benefit from proton therapy or altered RT?

## IV. REFERENCES

- Overgaard M, Hansen PS, et al. Postoperative radiotherapy in high-risk premenopausal women with breast cancer who receive adjuvant chemotherapy. Danish Breast Cancer Cooperative Group 82b Trial. *N Engl J Med* 1997; 337: 949-55
- Darby SC, Ewertz M, et al. Risk of ischemic heart disease in women after radiotherapy for breast cancer. *N Engl J Med* 2013; 368: 987-98
- C.R. Correa et al. Coronary artery findings after left-sided compared with right-sided radiation treatment for early-stage breast cancer. *J Clin Oncol*, 25 (2007), pp. 3031-3037
- O'Dell WG, Siva Kumar S, Determining prolate spheroidal modes of cardiac deformation directly from tagged heart images, 25th ISMRM Scientific Meeting and Exhibition, Honolulu, Hawaii, [#6447] April 2017.
- C. C. Moore et al., "Three-dimensional systolic strain patterns in the normal human left ventricle: characterization with tagged MR imaging," *Radiology* 214(2), 453-466 (2000)

## ACKNOWLEDGEMENTS

Funding for this work is from the Ocala Royal Dames Foundation for Cancer Research, University Scholars Program and the UF Foundation.